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## INHALER

This invention relates to dispensers for use with sol containers which contain medicaments for inhalation therapy, are pressurised with liquid propellants, and include a metering valve through which a series of metered medicament doses can be dispensed.

Inhalation activatable dispensers for use with 10 aerosol container assemblies of the type described above are known, their general purpose being to afford proper co-ordination of the dispensing of a dose of medicament with the inhalation of the patient thereby allowing the maximum proportion of the dose of medicament to be drawn 15 into the patient's bronchial passages. Examples of such dispensers are described in British Patent Specification Hos. 1,269,554, 1,335,378, 1,392,192 and 2,061,116 and United States Patent Hos. 3,456,644, 3,456,645, 3,456,646, 3,565,070, 3,598,294, 3,814,297, 3,605,738,

20 3,732,864, 3,636,949, 3,789,843 and 3,187,748 and German Patent No. 3,040,641.

European Patent No. 147028 discloses an inhalation activatable dispenser for use with an aerosol container in which a latch mechanism releasing wans is pivotally 25 mounted in an air passage between an aerosol outlet valve and a mouthpiece, which latch mechanism cannot be released if force to activate the dispenser is not applied before a patient inhales.

The dispenser generally comprises a housing having a 30 mouthpiece and an air passage therethrough terminating at the mouthpiece, the housing being adapted to receive an serosol container, said dispenser having a support block with a socket adapted to receive the stem of the walve of the serosol container and a through orifice communicating between the socket and the air passage, and latch means baving parts novable between an engaged position in which

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ent of the container and the support block toward each other upon the application of a force to bias the container and the support block toward each other is prevented and a release position in which movement of the container and the support block toward each other in response to said force is permitted causing the stem to move to its inner discharge position, the latch means comprising a wans mounted in the housing in the air 10 passagoway between the orifice and the mouthpiece for ment toward the mouthpiece under the influence of inhalation through the mouthpiece to release the latch means in which the wane moves toward the nouthpiece from a blocking to a non-blocking position with respect to the 15 passageway in response to inhaling at the mouthpiece and releases the latch means only during the application of said force to bias the container and support block toward each other.

This inhalation device has been received favourably 20 by patients and doctors since it not only overcomes the hand-lung co-ordination problem but it does so at a very low triggering flow-rate (approximately 30 litres/minute) essentially silently, and with a very compact design barely larger than a standard inhaler. It is necessary 25 to manually prime the inhalation device with a lever to apply the bias to the container prior to use.

U.S. Patent No. 4,648,393 discloses an electricallyoperated metered-dose inhaler in which a mechanical walve blocking means is withdrawn by the action of a solenoid 10 moving in response to the closing of a switch; the switch constitutes an electromechanical breath-actuation means which responds to inhalation by the patient. The disclosed device relies entirely upon mechanical priming of the device by application of force to a spring.

9087/04354 discloses a medical dosing device for the discharge of medicament for inhalation which comprises a

handheld holder for a medicine container from which medicine is discharged via a valve into an air channel for inhalation controlled by operation of an activation 5 device. The valve is operationally connected with a control unit arranged on initiation of the activation device to control the discharge valve for intermittant opening and closing repeatedly within an inhalation period. The control unit is an electronically controlled unit which activates an electrically controlled discharge valve.

It is an object of the present invention to provide an inhalation device for use with a pressurised earosol container equipped with a metered dose dispensing valve 15 which does not require manual actuation for firing the valve.

Therefore according to the present invention there is provided an inhalation device for use with a 20 pressurised acrosal canister containing a self-propelling sedicament composition equipped with a dispensing valve having a stem movable relative to the:canister between a closed position and a dispensing position, the device comprising a housing for supporting said canister and 25 maintaining the valve stem in a fixed position relative to said housing in communication with a patient port, the device additionally comprising electromechanical means for moving said canister thereby actuating the dispensing valve for administration of medicament.

The invention provides an inhalation device which removes the need for the patient to namually actuate the ecrosol valve by utilising electromechanical means, e.g., an electric motor or solenoid, to apply the required load for valve actuation to the aerosol canister or its associated valve ferrule. The provision of electromechanical means of valve actuation constitutes a

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Alternatively, the electromechanical means may be in the form of a solenoid which may be used to apply load directly to the serosol canister or via an intermediate 5 linkage to provide mechanical advantage in a similar manner to the linkages associated with an electric motor.

After actuation of the valve, the valve must be reset by returning the canister to its original position. The valve may be reset by returning the electromechanical 10 means to its original position and allowing the serosol canister to move under the influence of an internal spring within the walve, which is conventionally incorporated in all commercially available metared dose serosol valves. In one embodiment of the invention the 15 dispenser additionally comprises means for subsequently resetting the valve which may be operated by an electric notor or solemoid to drive the serosol canister back to its rest position. The motor or solenoid may conveniently be the same as that used for valve 20 actuation. The use of such reset means reduces the dependence upon the internal spring within the serosol valve and accordingly the valve may be provided with an internal spring of reduced strength, compared to those conventionally employed, such that it need only be strong 25 enough to return the aerosol valve to the reset position after pressure filling or function testing of the marcsol vial during namefacture. The strength of the valve spring is preferably selected so that a force of no greater than about 15% is required to effect actuation of 10 the device compared with a force of from 18 to 358 for conventional aerosol valves. Reducing the strength of the valve spring reduces the force required to actuate the valve and, in turn, reduces the power requirements of the notor or solemoid and the power and energy 15 requirements of the associated battery. Thus, the use of

significant benefit for those patients, generally children, the elderly and infirs, who may experience difficulty in manually firing an eerosol valve. A conventional serosol valve generally requires a force of from 18 to 15% to effect actuation. In a preferred embodiment of the invention the electromechanical means is associated with breath detection means such that the serosol valve is actuated automatically during inhalation by the patient, thereby overcoming any problems associated with potient hand-lung co-ordination.

The electromechanical means actuates the aerosol valve by applying a load either directly or indirectly to the aerosol canistar or its associated valve ferrule

15 whilst the valve stam is held stationary. Applying the load to the canistar in this way, rather than to the valve stam, has the important advantage of keeping the support block which houses the spray exit crifice stationary thereby obviating the need to move the

20 mouthpiece in unison with the support block during actuation to ensure that the medicament is always dispensed to the same area in the mouthpiece and that dosage reproducibility is efficient.

An electric motor may be used to apply the load to
the canister by numerous different arrangements. For
example, the motor may drive through a wors gear attached
to a threaded component which acts directly on the base
of the aerosol canister. Actuation of the motor in one
direction causes advance of the threaded component moving
the aerosol canister to actuate the valve. In other
embodiments of the invention one or more intermediate
linkages are provided to achieve greater mechanical
advantage. For example, a lever which is driven via a
wors gear, a can or suitable gear train may be utilised
to apply the load to the canister.

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valves having weak valve springs is a significant advantage in the design of pressurised inhalers having electromagnetic valve actuation and reset. The use of 5 valves having weak springs and being reset by an electric motor or solenoid requires the valve stem to be hald in position in the nozzle block.

Preferred inhalation devices in accordance with the invention additionally comprise means for detecting inspiration through the patient port associated with control means for actuating the device on detecting of inspiration. Such a breath actuation means may comprise a simple pivoted vane which noves to close an electric switch when the patient inhales through the patient port or may comprise other means for detection of inhalation, e.g., based upon change in temperature or pressure which provides a signal used to initiate activation of the electromechanical means to activate the valve. Other suitable means for detection of inhalation include flow memorrs e.g. those which measure the speed of rotation of a turbine in the air stream.

Smitable inhalation devices are disclosed in our copending British Patent Application of evan date entitled
25 "Inhalation Device" and comprise a portable inhalation
device for administration of medicament in the form of
aerosolised fine particles or droplets of liquid or
suspension to the respiratory system of a patient, the
device comprising a housing defining a chamber in
10 communication with a patient port in the form of a
monthpiece or masal adaptor, medicament aerosolisation
means for forming an aerosol of medicament in the
chamber, control means to actuate the medicament
aerosolisation means and a sensor which measures the air
15 flow rate during respiration through the patient port and
provides an electrical signal to the control means which

varies continuously with said flow rate, said electrical signal being used by the control means for one or more of the following functions:

- (i) to calibrate the device such that the medicament aerosolimation means is actuated at a precise, pre-determined flow rate,
- (ii) to monitor one or more of the following parameters:
- (a) flow rate at different times during respiration.
  - (b) rate of change of flow rate during respiration,
  - (c) respired volume during respiration,

and activate the medicament perceolisation means when a 15 pre-determined inspiration parameter is attained.

The electromechanical breath actuated inhalars of the invention eliminate the need for manual actuation or prining of the device and avoid the need for a blocking mechanism to prevent firing of the valve which are 20 required in devices where the mechanism is primed prior to breath actuation. In the devices of the invention, upon detection of the start of inhalation, or the attainment of some inhalation parameter, the motor or solenoid is energised and the load immediately applied 25 to the serosol canister causing the serosol valve to

The inhalation device of the invention may also include other electronic control features, e.g., to provide an indication of the number of doses dispensed or 30 remaining, or to control the dosage frequency. For example, the device may include electronic control means such that the aerosol valve cannot be fired for a predetermined period of time after a dose has been dispensed in order to ensure the patient does not take a further 35 dose before the initial dose has had time to take effect.

The control means may also provent dispensing from the

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Figures 9 and 10 represent side and front sections respectively through an inhalation device in accordance with the invention.

Back of Figures 1 to 8 illustrate an inhalation davice comprising a housing (2) baving a patient port (4) in the form of a mouthpiece. The device comprises a nozzle block (6) which is fixed relative to the nouthpiece. A pressurised corosol vial comprising an ..10 serosol canister (8) equipped with a valve having a valve stem (10) is enclosed within the housing and arranged such that the valve stem (10) is firmly secured within the noise block (6). Howement of the serosol canister (8) in the downward direction causes actuation of the 15 valve dispensing medicament through the nozzle block (6) into the mouthpiece (4) for inhalation by the patient.

In any of the inhalers shown in Figures 1, 2, 3, 4 and 5 the notor could have associated with it a gearbox.

Referring to Figure 1 the electromechanical means 20 for poving the aerosol canister (8) to fire the valve comprises a notor (12) attached to the housing (2) to prevent rotation which rotates a screw thread (14) passing through a threaded aperture on actuation lever (16). Activation of the notor rotates the screw thread 25 (14) causing the actuation lever (16) to move downwards thereby moving the serosol canister (8) and firing the valve (4). Vertical translational motion of the actuation lever (16) is ensured by two lugs (17), only one of which is shown, which engage complimentary 30 vertical slots (not shown) in the wall of housing (2) thereby preventing rotation in any plane.

The device additionally comprises a second screw thread (18) passing through a threaded sperture on a valve reset arm (20) extending beneath the valve ferrula. When the motor is actuated to fire the valve the screw (18) is rotated causing downward movement of the reset

device if the patient has received the maximum mum doses within a pre-determined period of time in order to prevent patient overdose. In addition, the control means 5 may also provent further dispensing from the device when a predetermined number of doses indicated on a label have already been taken, thus preventing "tail off" problems leading to reduced domes of medicament being dispensed. Since the electromechanical means would only be energised 10 mean demand if so directed by the electronic control means the possibility of valve actuation when not permitted may be completely eliminated by ensuring the canister bese and other internal components are inaccessible, thereby preventing unauthorised petient tampering etc.

The electronic control means may also control the valve resetting to ensure that the valve is reset under optimum conditions. Ideally, the valve should be reset immediately or shortly after valve actuation to ensure 20 the device is set ready for the next use. Such immediate resetting greatly reduces or eliminates the possibility of vapour-lock formation in the valve which can occur if the valve is left in its fired state for a significant length of time or is allowed to reset who 25 the aerosol container is not hald in the upright position. In addition, the control means for valve resetting may include a tilt-detection means which provides a warning to the patient to hold the container vertically in order to prevent a vapour-lock occurring if 30 the valve is reset when the aerosol canister is tilted and the liquid medicament therein is not in contact with the valve.

The invention will now be described with reference to the accompanying drawings in which:

Figures 1 to 8 represent schematic diagrams of inhalation devices in accordance with the invention and.

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arm (20) to allow movement of the aerosol canister (8). Rotation of reset arm (20) is similarly prevented by two interengaging lugs/slots (not shown). When the valve is 5 reset the motor is rotated in the opposite direction causing actuation lever (16) to return to its rest position and the reset arm (20) is raised with the serosol camister (B) upwardly to its rest position.

The device may be actuated by nammal pressing of a 10 button (not shown) or by electrical inhalation detection circuitry (not shown). Actuation of the reset cycle may be initiated by manual pressing of a reset button, by electrical detection means which detects the cossetion of patient inspiration, by a switch actuated on replacement 15 or closing of a mouthplace cover or after a preset time delay following actuation of the valve or immediately after the device has fired, or a combination of the ab (e.g. preset delay after cossation).

The electromechanical means for moving the canister 20 of the device shown in Figure 2 comprises a motor (22) attached to the housing (2) to prevent rotation which drives a screw (24) associated with a combined actuation driver (26) and reset arm (28). During actuation rotation of the screw (24) causes the actuation driver 25 (26) to move downwardly causing corresponding movement of the aerosol canister to fire the valve. Rotation of the combined actuation driver/reset arm is prevented by lugs (29) Which angage complimentary vertical slots or grooves in the wall of the housing. The reset arm (28) moves 10 with the actuation driver and the valve is reset by driving the notor in reverse. Actuation of the valve and reset may be initiated by similar means to those discussed with reference to Figure 1.

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With reference to Pigure 3, the electromechanical means for moving the aerosol canister comprises a motor (30) attached to the bousing (2) to prevent rotation which drives a screw (32) associated with a combined actuation driver (34) and reset arm (36) which are positioned either side of the Valve farrule (38) and are prevented from rotating with the screw. When the motor is activated to rotate the screw (32) the actuation 10 driver (34) and reset arm (36) move downwardly causing povement of the serosol canister (8) to fire the valve. The motor is then driven in reverse, returning the actuation driver and reset arm to the rest position causing upward movement of the canister (8) to reset the 15 valve. Alternatively, the reset arm (36) may be eliminated, both valve actuation and reset being performed by driver (34). Actuation of the firing and regetting cycles of the valve may be arranged as discussed with reference to Figure 1.

Referring to Figure 4, the electromechanical means for moving the canister is similar to that shown in · Figure 3 and comprises a motter (40), screw (42), actuation driver (44) acting on the valve ferrule (48) and a resat lewer (46) which is connected to the 25 actuation driver (44) at pivot (47). Two lugs (45) are provided to prevent rotation of the actuation driver (44) as described above for the device shown in Figure 1. The valve firing and resetting cycles operate as described with reference to Figure 3.

The electromechanical means for moving the serosol canister in the device shown in Figure 5 comprises a otor (50) having a shaft (52) which is attached to a cam (54). The surface of the cam (54) acts on actuation driver (56) such that when the can is rotated the 35 actuation driver is caused to move downwardly, ir turn causing down movement of the aerosol canister (8) to fire

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the device housing at (81). When the device is actuated by energiaing the solemoid the plunger (72) moves downwardly pulling the actuation lever (74) which in turn 5 causes downward movement of the serosol canister (8) firing the valve. The two pivot points (77, 81) are chosen so that the reset arm (78) moves downwardly during the actuation cycle allowing free movement of the aerosol canister and when the solenoid is de-energised the 10 plunger returns to its rest position causing upward ment of the actuation lever (74) and reset arm (78) noving the serosol canister (8) to its rest position thereby resetting the valve. The initiation of the valve firing cycle may be conducted as described with reference 15 to the device illustrated in Pigure 1.

Referring to Figure 8 the electromechanical mean for poving the aerosol canister (8) comprises a solemoid (80), plunger (82) which is connected to cam (84) by a pivoted linkage (86). The can (84) rotates about (85) to act on an actuation driver (88) which is positioned at the base of the aerosol canister (8). When the solenoid is energised, the plunger moves upwardly and the pivoted linkage (86) causes the can (84) to rotate pushing the actuation driver (88) downwardly causing movement of the 25 serosol canister (8) to fire the valve. When the solenoid is de-energised and the plunger returns to its rest position causing rotation of the can to its rest position the aerosol canister (8) and the actuation driver (88) are moved upwardly under the influence of the 30 internal spring of the aerosol valve.

Piqure 9 shows an imbaler (100) with a hinged nouthpiece cover (102) which can be opened to reveal a patient port in the form of a routhpiece (104). The outhpiece has attached to it a nozzle block (106) and the mouthpiece/norsale block are removable for cleaning

the valve. Stop (57) on the can and stop (58) on the actuation driver are provided to halt rotation of the cam when the required movement of the serosol canister has 5 been completed. Alternatively, a stepper motor could be used, thereby possibly obviating the need for a separate de-energising switch. The stops may act as a switch to de-energise the motor. The valve reset is achieved by driving the notor in reverse and either noving the canister upwards or allowing the serosol canister to move upwardly under the influence of the internal spring of the aerosol valve.

Referring to Figure 6 the electromechanical means for moving the serosol canister (8) comprises a solenoid (60) and a plunger (62) connected to a combined actuation driver (64) and reset arm (66) which act on either side of the valve ferrule (67). When the solenoid is energised the plunger moves downwardly causing downward movement of the actuation driver, valve reset arm and serosol canister causing the valve to fire. The solenoid is do-energised and the plunger returns to its rest 'position under the influence of the solenoid return spring causing upward povement of the actuation driver, valve reset arm and serosol canister to its rest 25 position. Alternatively, the reset arm (66) may be eliminated, both valve actuation and reset being performed by driver (64). The firing and reset cycles of the valve may be initiated in the manner described with reference to the device illustrated in Figure 1.

Referring to Figure 7, the electromechanical means for moving the aerosol canister (8) comprises a solenoid (70) having a plunger (72) connected to an actuation arm (74) at pivot (75). Actuation arm (74) pivots about (77) to act on the base of the agrosol canister (8) thereby 35 generating mechanical advantage. A reset arm (78) is connected to end (76) of the plunger at pivot (79) and to

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Inserted into the nozzle block is the valve ston (108) of a metered dose inhaler (110). The metered dose inhaler will be referred to as an MDI. The valve stem is prevented from moving down with respect to the nozzle block by a small projection (112) formed as part of the nozzle block. However, there is sufficient space (114) in the mossic block to allow the remaining parts of the walve (116) to travel downwards during the action of 10 'firing' the MDI.

The holes (122) in the rear of the device serve as air inlets when the patient inhales on the mouthpiece.

The battery (124) can be accessed through a cover (126) in the back of the device.

Most of the electronic components of the device are on a circuit board (128), this could take the form of a printed circuit board or, to save space, an ASIC for example (i.e. an application specific integrated circuit).

Picture 10 shows a front section of the firing mechanism in more detail. The can (130) takes the form of a short cylindrical block pounted eccentrically ontothe output spindle (132) of a reduction gearbox (134). The can is mounted within a housing (136) which is free 25 to move up and down with respect to the HDI. The can and housing are preferably made from similar materials to pininise wear.

A d.c. notor (138), which could be continuous or of the 'stepper' type, is mounted onto the gearbox so that 30 the notor output drives the gears (not shown). The gears are arranged such that the angular valocity of the motor (typically around 13000 rpm) is reduced to give one revolution in approximately 0.2 to 0.5 seconds. Also attached to the gearbox is a nicro-switch (140), with its actuator arm (142) resting on the top of the bousing

The whole of the firing mechanism is attached to the body of the device (144) by four tension springs (146 to 149) which are attached at one end to a cross-number 5 (150) which bears down on the gearbox and at the other and to the device body.

The operation of the device will now be described.

The patient must first shake the device to mix the
contents of the serosol can and must assure that the
10 mouthpiece cover is open and the air intakes are clear.

The patient inhales on the nouthpiece, setting up a flow of air into the intakes (122) and through the empty region (152) of the inhaler. The air travels through channels in the nozzle block to either side of the spray 15 outlet and thereafter out through the nouthpiece. (The nozzle block (106) forms a sufficiently good seal with the nain body of the device that the preferential path for the air is from the intakes to the nouthpiece).

Ehilst still inhaling, the patient must press a
switch (not shown) to operate the electro-mechanical
firing mechanism. When the switch is depressed the motor
is made to turn until the cam has made one complete
revolution. As the can turns, it presses downwards on
the housing (116) which in turn presses down on the base
of the aerosol can. Since the valve stem cannot move
with respect to the norsile block, which is attached to
the body of the device, the net result is that the valve
stem is pushed up into the aerosol can thereby firing the
MDI and releasing medicament in the normal way.

When the cam returns to the top of its traval the housing contacts the actuator (142) of the micro-switch (140), sending a signal to the electronics to stop the

The diameter of the can and the point at which it is 15 mounted, are arranged such that at the bottom of its travel the can has caused the valve to be compressed by

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 An inhalation device for use with a pressurised earosol canister containing a self-propelling medicament composition equipped with a dispensing valve having a stem movable relative to the canister between a closed position and a dispensing position, the device comprising a bousing for supporting said canister and maintaining the valve stem in a fixed position relative to eaid bousing in communication with a patient port, the device additionally comprising electromechanical means

to said housing in communication with a pattern port, and device additionally comprising electromechanical means for moving said canister thereby actuating the dispensing valve for administration of medicament. 2. An inhalation device as claimed in Claim 1 in which

- an innatural valve is a metered dose dispensing valve.
   he dispensing valve is a metered dose dispensing valve.
   he inhalation device as cleined in Clain 1 or Clain 2 in which the electromechanical means for moving the serosol canister comprises an electric meter or solenoid connected by a driver arrangement to an actuation driver which acts on the serosol canister or valve ferrule to
- move the serosol canister when the electric motor or solenoid is energised. 4. A device as claimed in Claim 3 in which the driver
- arrangement comprises a screw.

  25 5. A device as claimed in Claim 3 in which the driver
- arrangement comprises a can.

  6. A device as claimed in any preceding Claim which
- additionally comprises a reset number which acts on the serosol canister or valve ferrule, the reset number being driven by an electric motor or solenoid or solenoid
  - apring to return the aerosol canistar to a reset position closing the dispensing valve. 7. A device as claimed in Claim 6 in which the electric
- notor or solenoid or solenoid spring driving the reset
  senser is the electric notor or solenoid or solenoid
  spring driving the actuation driver.

more than the minimum amount necessary to properly fire the MDI. In case the cas is arranged such that the valve compression would exceed the maximum permitted travel, 5 the whole of the firing mechanism can lift, against the action of the four springs, to ensure that the can is always able to make a full rotation without stalling. Thus, the strength of the springs must be arranged so that, when acting in unison, they are sufficiently strong 10 to allow the valve to compress normally without

extending, but sufficiently weak as to allow the

nechanism to lift if the valve 'bottoms out'.

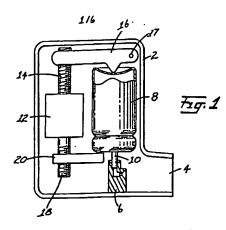
In a preferred variation of this embodiment the device would be made breath activated by incorporating a 15 muitable flow mensor into the space (152). In this case the patient would press a button to turn the electronics on, or a switch could be incorporated in the mouthpiece cover and the electro-mechanical firing mechanism would then be operated automatically as soon as the appropriate

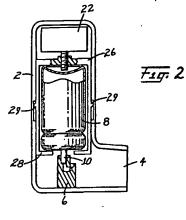
20 triggering flow rate or inhalation parameter was detected. Suitable breath sensors are disclosed in the prior art referred to herein and in our co-pending British Patent Application No. 9023282.8 and the PCT Application of even date based thereon, the disclosures

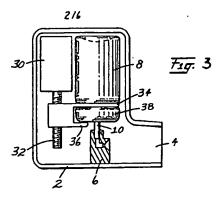
25 of which are incorporated herein by reference.

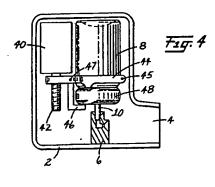
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- A device as claimed in Claim 6 or Claim 7 comprising control means to actuate the valve reset member after firing the valve.
- 5 9. A device as claimed in Claims 6 to 8 which additionally comprises indicating means to prevent valve reset if the canister is not substantially vertical or to warn the patient to hold the canister in a substantially vertical position.
- 10 10. A device as claimed in any one of Claims 6 to 9 in which the dispensing valve comprises a spring binading the valve stem to the closed position, the strength of the spring being selected so that a force of no greater than 15N is required to effect actuation of the device.
- 15 11. A device as claimed in any preceding Claim which additionally comprises means for detecting patient inspiration through the patient port and control means for actuating the electromechanical means for noving the serosol canister in response to detection of patient 20 inspiration.
  - 12. A device as claimed in any preceding Claim which additionally comprises control means to control the desage frequency by preventing actuation of the electromechanical means for a pre-determine pariod of the control desage of a number of desage of
- 25 time after dispensing a dose or a number of doses of medicament.
  - A device as claimed in any preceding Claim which additionally comprises control means to prevent actuation of the electromechanical means after a predetermined
- 30 mmber of doses of nadicassant have been dispensed from the device.
  - 14. An aerosol device as claimed in any preceding Claim containing said pressurised aerosol canister equipped with a dispensing valve.
- 35 15. A method of edministering a medicament using an marpsol davice as claimed in Claim 14.









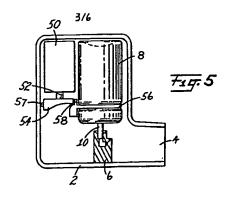
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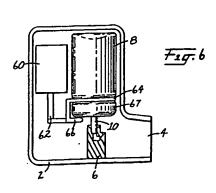
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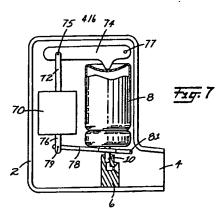
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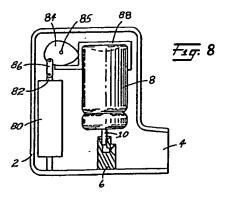
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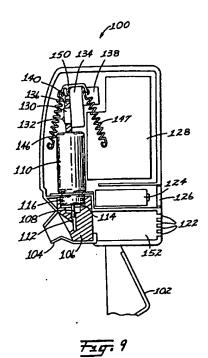




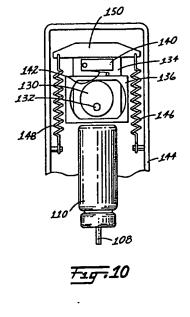


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